BIOMATERIAL SURFACES: MODIFIED TITANIUM SURFACES AND MICROFABRICATED MATERIALS

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Most "biomaterials" in use today were originally developed for other applications than biological. The tissue responses they give rise to are often far from optimal. One major bottle-neck for developing new and better (functional) biomaterials is the lack of understanding of how different material properties influence the biological response and vice versa.

The material-specific biological response to an implanted material is mainly determined by the chemical and structural properties of the biomaterial surface [1]. Research on properties and processes at interfaces between biomaterial surfaces and biological systems is therefore a key issue in the biomaterials area. A systematic research approach should include surface modification by different preparative techniques combined with careful surface characterization using modern analytical tools, to produce well-defined model surfaces which can be used in biological evaluation studies in vitro and in vivo (Fig. 1). Biological evaluation can be done at different levels of complexity, including simple model experiments of water, ion and biomolecule adsorption, cell cultures, and tissue response in vivo. Such an interdisciplinary research program opens up a way to systematically search for correlations between different surface properties and biological response. Two models systems based on these ideas are briefly described, with emphasis on the surface preparation and analysis aspects.



Fig. 1 - Research approach where surface preparation and analysis are combined to prepare model surfaces that are used in biological evaluation studies aiming at finding correlations between surface properties and biological response.

Systematic Modification of Scheice Properties for Stedning Biological Response

Modified Tetanium Surfaces

Tanaium is a unitable material for undying material-sious interaction for you major tensors. Oil is widely and accountily used in secred divide algorithm on the first and the proposal content (see all mining and the proposal content (see all mining and the secred and in a proposal content (see all mining and the secred and in surface properties can be modified over a wide range. Despite its wide use in clinical applications see factors and mechanisms that underline the tissue response to titarium implants are poorly understood. It is, bootever, likely that the surface coids which almost always covers the material para important role. The question is then How do different orde properties (e.g. influences microstructure, crystallines, chemical composition, importion, ...) influence the biological response to titarium? The devision approach to investigate this is to vary the surface (coids) proporties and test for the response in different biological experiments (protein adsorption, cell cultures, and animal contribution).

We have carried our a bound characterization, using surface spectroscopies AES, XPS/ESC, SINS), electron microscopies (SEM, 17EM) and scanning antoprobles (STM, AFM), of I surfaces prepared by different methods funching, thermal oxidation, electrochemical methods, and glow-discharge plasma methods) (2-8). This work has resulted in a good understanding of bow different preparative procedures influence the physical and chemical properties of IT surfaces. Selected results from such studies are bettely summarized in Table 1. The table also demonstrates that the properties of IT surfaces can be modified over a wide range. Different modified II in of bowe response in vivo (4). The faces of the contraction of the

Microfabricated Model Materials

	Parameters	Thickness	Composition	Structure	Impurities	Dopani
"Clinical" oxides	Machining, cleaning, sterilization, handling	2-6 mm	TiO ₂ + sub-oxides (Ti ₂ O ₃ , TiO) + small amounts of TIN ₄	Quesi- amorphous, dense	C. Ca. P. St. Cl. S. Na at %- levels.	
Thermal oxides	Temperature, pressure, time, oxidizing gas (O ₂ , O ₃ , H ₂ O)	10 - 40 nm	TiO ₂ + sub-oxides (= OH in faumid atmospheres)	Quasi-amorphous to crystalline (anatase or rutile)	Depends on gas composition	
Anodic oxides	Anode voltage, electrolyte, temperature,	Up to several microns (µm)	TiO ₂	Quasi amorphous to crystalline, heterogeneous, dense to porous	Anions from electrolytes, (SO ² , PO ²)	Anions (-1%)
Plasma oxides	Plasma gas coreposition and pressure, sample voltage, temperature, time	Up to several 100 nm	TiO ₂ , variable	Quasi-amorphous to crystalline, idense	None (but care in handling is important)	Almost
Electro- polished Ti	Electrolyte, temperature, time.	3-5 nm	по,	Quasi-amorphous	a	
Alloyed TI, TIGAI4V	Bulk metal composition, and as above	As for pure Ti	TIO ₂ + % levels of AIO ₄ and VO ₅	As for pure Ti	Al, V, and as above	As for pure Ti

Table

influence the interaction with biomolecules, while structures and/or chemical variations on the $1-10~\mu m$ scale will influence cellular behavior at surfaces.

In our group we have adapted the methods that are used in fabrication of microelectronic devices — mierofabrication and manifabrication based on lithography, exching and thin fills deposition — for preparing model surfaces for biological evaluation that have variations in chemical composition and/or microstructure on well-defined size scales (Fig. 2). This type of surfaces oftel unique possibilities to study how biological response at different levels are influenced by surface structures and chemical composition.

Microfabricated model surfaces have been used, for example, for studyine the influence of chemical composition on the adhesion and colonization of Staph. Epidermidit bacteria in the Ti-Al-V metal system [11]. The choice of the Ti-Al-V metal system [11] the choice of the Ti-Al-V metal system was in this case motivated by the wide-spread use of the Ti-Al-V metal system was in this case motivated by the wide-spread use of the Ti-Al-V metal system and the missage could be the three contents of the missage could be the system of the missage could be supported by the system of the system o

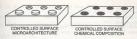


Fig. 2 - Schematic illustration of microfubricated model surfaces for studying biological responses to variations in surface structure and/or chemical composition. Feature sizes may be varied in the range from a few 10 mm up to hundreds of microns.

surfaces with a preference following the order V > Ti > Al [11]. Microfabricated model surfaces with well-defined surface structures on the 10 µm level are also presently used in studying macrophage responses in vitro.

CONCLUDING REMARKS

Biomaterials is an extremely complex field and its advancements requires interdisciplinary approaches. The area offers many challenges and opportunities for materials scientists. Modern preparative and analytical methods from surface science are particularly useful, since they open up a way to systematically investigate relationships between material surface properties and biological response.

Most biomaterials in use today give rise to non-optimal tissue responses which are difficult to prediet and control. The current trend in biomaterials research is to attempt to develop more active biomaterial surfaces which have specific surface properties designed to give a desired dissue response. Such future biomaterials will most likely be sophisticated materials, produced by a formation of high-tech materials preparation techniques and methods from consideration of high-tech materials preparation techniques and methods from

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